

# DEVELOPMENT OF WEARABLE GAIT ANALYSIS DEVICE BASED ON VERTICAL GROUND REACTION FORCES

By

**Nuramerica Deni<sup>1</sup>, Muhammad Hazli Mazlan<sup>1,2</sup>, Ida Laila Ahmad<sup>1,2</sup>, M. Anas Razali<sup>1</sup>, Mohd Khairul Ahmad<sup>1,2</sup>, Nur Dalilah Diyana Nordin<sup>3</sup>**

<sup>1</sup>Faculty of Electrical and Electronic Engineering, Universiti Tun Hussein Onn Malaysia, Malaysia, mhazli@uthm.edu.my

<sup>2</sup>Microelectronics and Nanotechnology-Shamsuddin Research Centre, Universiti Tun Hussein Onn Malaysia, Malaysia, mhazli@uthm.edu.my

<sup>3</sup>Information Technology Centre, Universiti Tun Hussein Onn Malaysia, Malaysia, dalilah@uthm.edu.my

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# INTRODUCTION

- Gait analysis is the assessment of the walking pattern.
- Biomechanical analysis of a gait pattern employs various methods such as kinetic analysis, pressure measurement, dynamic electromyography, etc.
- **The purpose of gait analysis system development:**
  - i. To measure the degree of pronation which the natural inward rolls act as a shock absorber for the leg and body by optimally disturbing the force of the impact when the heel hitting the ground
  - ii. To analyse the gait variability for monitoring or analyzing the gait pattern that can be used for therapy
  - iii. To detect any abnormalities of the gait cycle at early stage

# Problem Statements

- In the field of biomedical engineering, gait analysis has been a fundamental method and assistive tool to characterize human locomotion.
- A standard gait analysis method has been successfully developed and applied in a number of gait laboratories – **requires specialized labs, expensive equipment, a long-time processing and a large area to perform the experiment**
- To overcome this problem, an alternative gait analysis method based on wearable sensors, which can be used outside the laboratory environment has been introduced in this study.

# Objectives

1. To develop a wireless hardware and devices for a gait analysis system based on vertical GRFs.
2. To analyse the performance of the developed device by comparing the gait pattern obtained from the device with the standard gait data.

# PROJECT DEVELOPMENT

This project consists of two main parts:

## 1) Hardware part

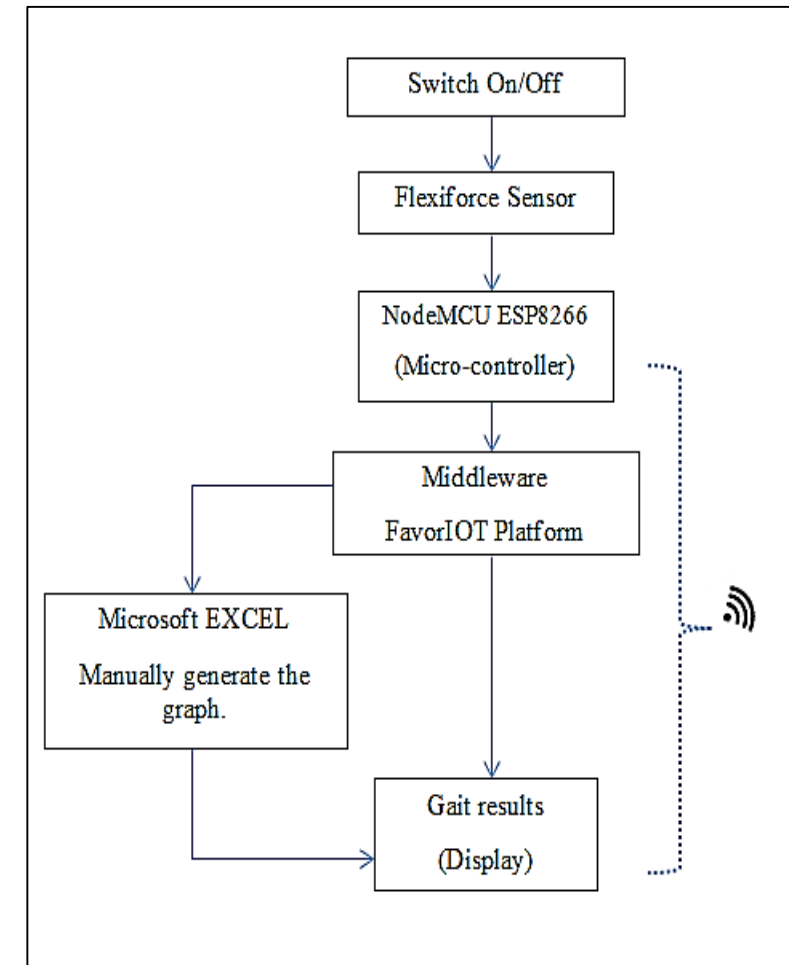
### **Sensor** - Flexiforce Sensor (FFS):

- Used to record the pressure generated
- High durability, lightweight, small size and easy to embed on the shoes.

### **Micro-controller** - NodeMCU (ESP8266):

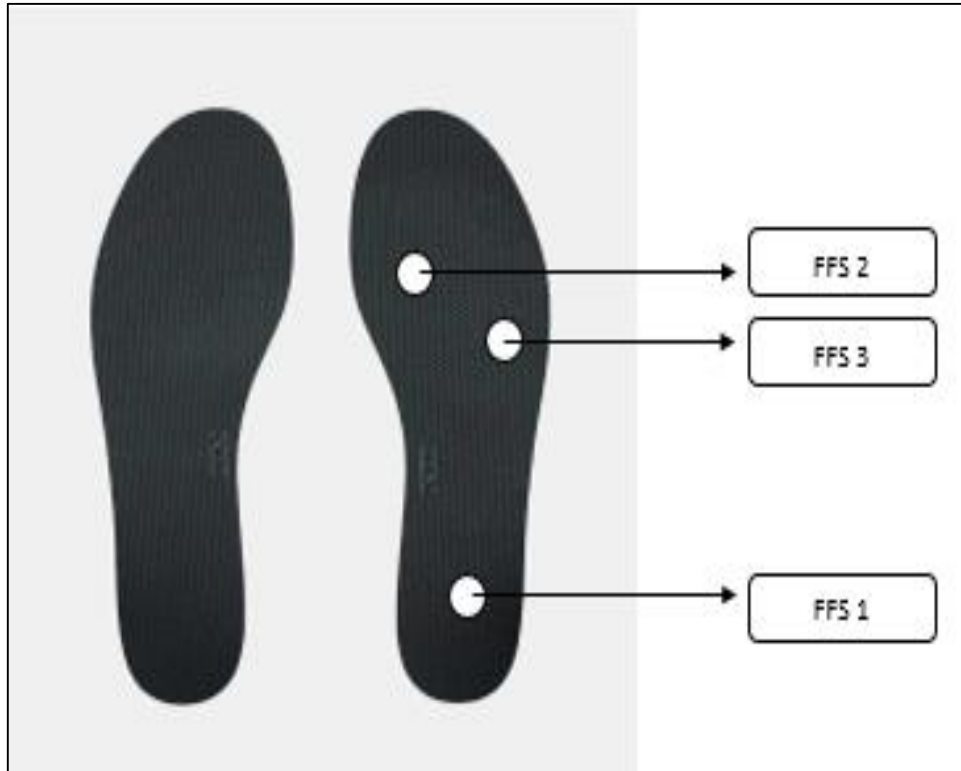
- Wireless capability and small size

## 2) Software part – Arduino IDE



Block diagram of the project

# PROJECT DEVELOPMENT



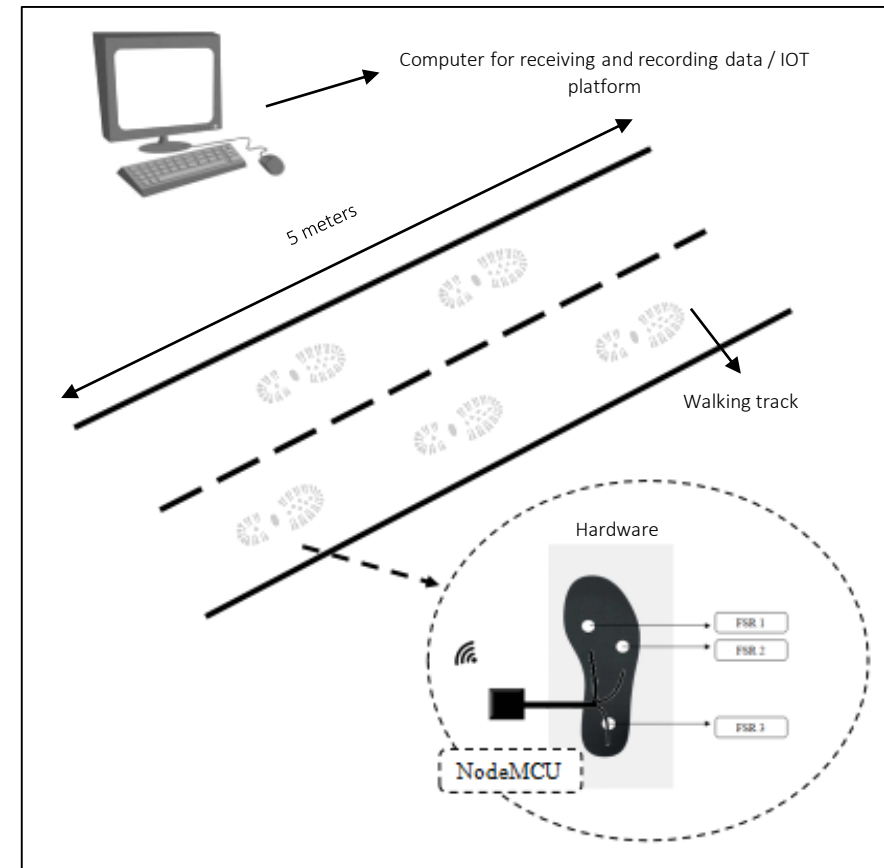
Pressure sensor locations



Hardware final design

# EXPERIMENTAL SETUP

1. The analysis was conducted based on the designated walking track.
2. The walking track was set to 5-meter in length – considered the limited space on the lab and the subject able to produce at least two complete gait cycle (1.5 m per stride).
3. The subject was asked to walk in a normal working pace.



Experimental setup (walking track)



# EXPERIMENT PROCEDURE

**Step 1:** The subject need to read and fill in the consent form.

**Step 2:** Record the name and weight of the subject.

**Step 3:** Prepare the insole to the subject. The insole must be properly worn by the subject.

**Step 4:** Check the walking track and make sure it is clear from any hazards.

**Step 5:** The subject walk on the track provided for every step in 2 minutes.

**Step 6:** The data obtain saved and displayed in the computer.

**Step 7:** Analyse the results.

# DEMOGRAPHIC INFORMATION

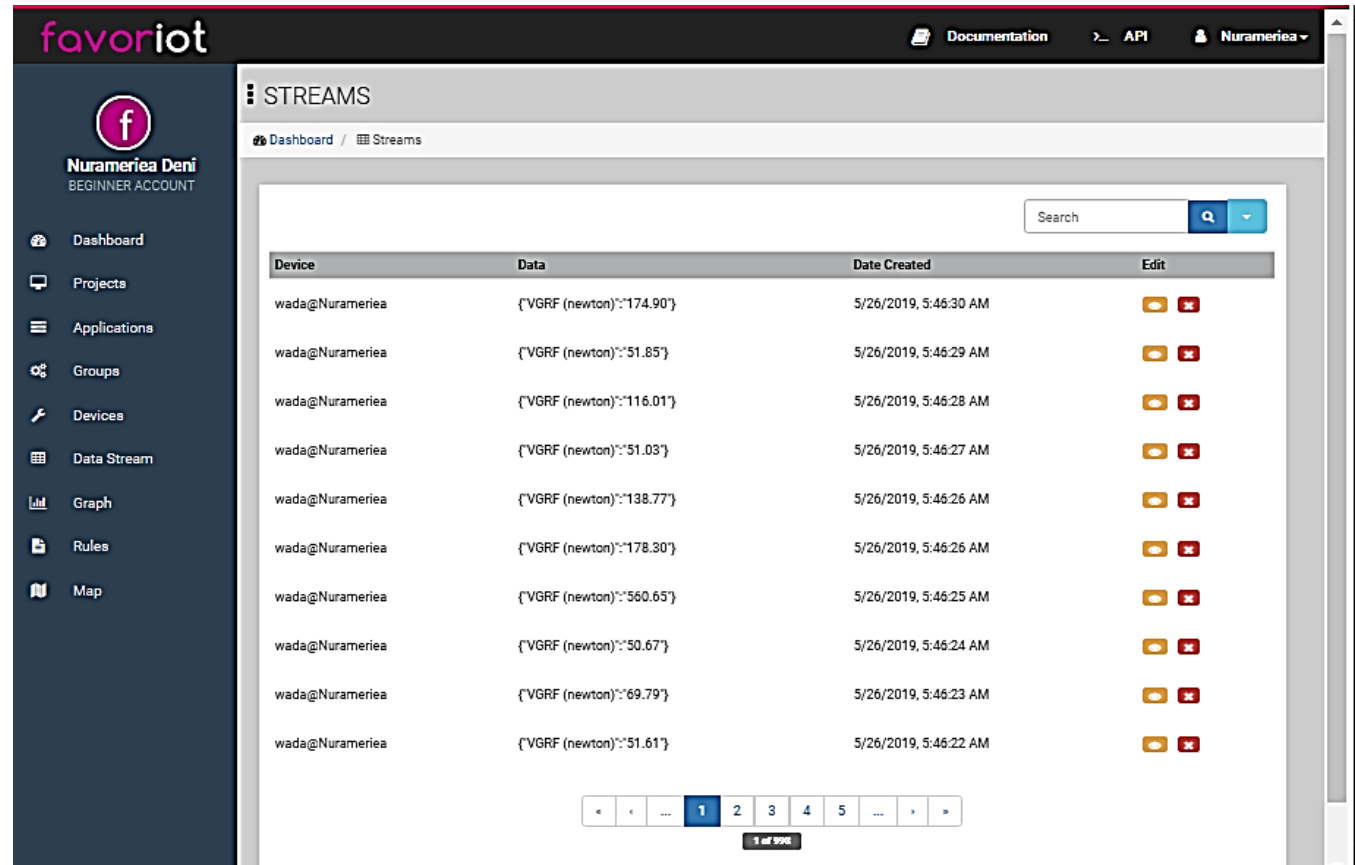
- The difference in the subjects' body weights can greatly influence the force and gait pattern during walking – the criterion can be used to validate the results of the study.

No	Name	Age	Gender	Weight (kg)
1.	Subject 1	26	Female	38
2.	Subject 2	26	Female	47
3.	Subject 3	27	Male	83
4.	Subject 4	27	Male	80
5.	Subject 5	26	Female	56
6.	Subject 6	27	Male	72
7.	Subject 7	27	Female	96
8.	Subject 8	26	Female	43
9.	Subject 9	26	Female	85
10.	Subject 10	24	Female	45





















Demographic information of the subjects

# DATA STREAM ON FAVORIOT

- The data obtained from the force sensors was sent wirelessly to the computer.
- The FavorIOT platform allows user to directly access the data without requiring manual data transfer from a memory card.



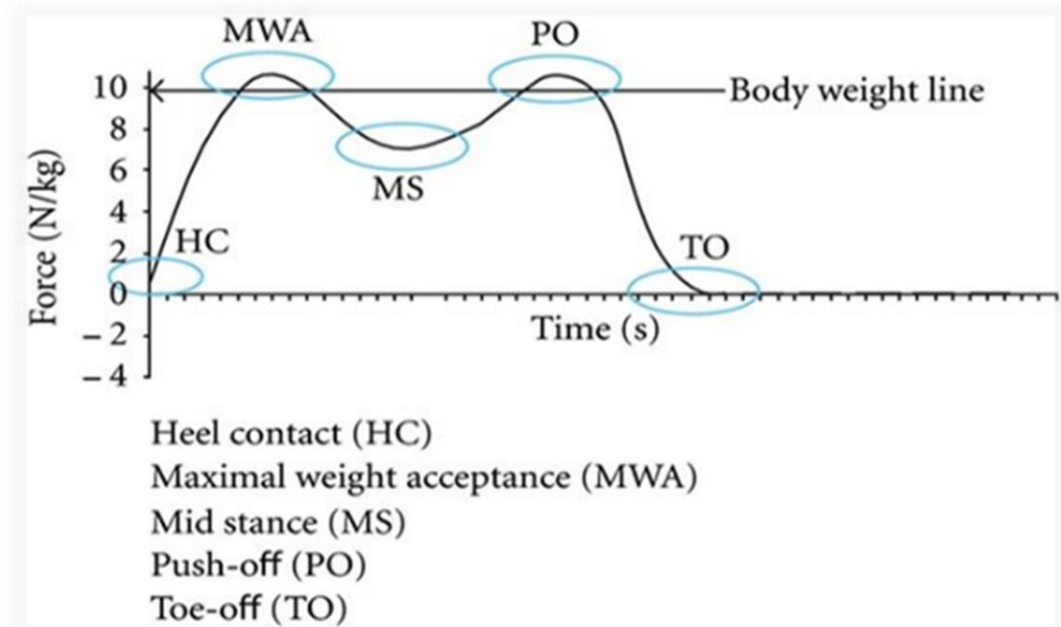
The screenshot shows the FavorIOT web interface. The left sidebar contains navigation options: Dashboard, Projects, Applications, Groups, Devices, Data Stream, Graph, Rules, and Map. The main content area is titled 'STREAMS' and displays a table of data points. The table has columns for Device, Data, Date Created, and Edit. The data points are for a device named 'wada@Nurameriea' and represent force sensor readings in Newtons.

Device	Data	Date Created	Edit
wada@Nurameriea	{'VGRF (newton)':174.90}	5/26/2019, 5:46:30 AM	 
wada@Nurameriea	{'VGRF (newton)':51.85}	5/26/2019, 5:46:29 AM	 
wada@Nurameriea	{'VGRF (newton)':116.01}	5/26/2019, 5:46:28 AM	 
wada@Nurameriea	{'VGRF (newton)':51.03}	5/26/2019, 5:46:27 AM	 
wada@Nurameriea	{'VGRF (newton)':138.77}	5/26/2019, 5:46:26 AM	 
wada@Nurameriea	{'VGRF (newton)':178.30}	5/26/2019, 5:46:26 AM	 
wada@Nurameriea	{'VGRF (newton)':560.65}	5/26/2019, 5:46:25 AM	 
wada@Nurameriea	{'VGRF (newton)':50.67}	5/26/2019, 5:46:24 AM	 
wada@Nurameriea	{'VGRF (newton)':69.79}	5/26/2019, 5:46:23 AM	 
wada@Nurameriea	{'VGRF (newton)':51.61}	5/26/2019, 5:46:22 AM	 

Data stream on FavorIOT platform

# STANDARD VGRF DIAGRAM

- The results were evaluated by referring to the standard diagram of VGRF for normal gait, Bouffard et al.
- Five significant events of gait – heel contact (HC), maximal weight acceptance (MWA), mid stance (MS), push-off (PO) and toe-off (TO).
- To determining and assessing the gait pattern of individual.



**Vertical ground reaction force (GRF),**  
 Bouffard et al.

# GAIT DATA ANALYSIS

- The vGRF value and percentage of gait cycle was calculated using the formula in equation (1) and (2):

$$V_{grf} = \frac{\text{Output value (N)}}{\text{weight of subject (kg)}} \quad (1)$$

$$\% \text{ gait cycle} = \left( \frac{\text{time(s)}}{\text{total time (s)}} \right) \times 100 \quad (2)$$

# RESULTS – GAIT DATA

Time (s)	Subject 1 (N)	% Gait Cycle	vGRF (N/Kg)
0	63.05	0.0	1.66
1	407.32	16.7	10.72
2	311.9	33.3	8.21
3	260.76	50.0	6.86
4	388.71	66.7	10.23
5	58.42	83.3	1.54
6	0	100.0	0.00

Complete gait cycle data of Subject 1

Subject	Standard value (N/kg)	Device reading (N/kg)	Percentage difference (%)
1	1	1.05	5
2	1	1.09	9
3	1	0.98	2
4	1	1.06	6
5	1	0.92	8
6	1	1.03	3
7	1	0.96	4
8	1	0.92	8
9	1	0.96	4
10	1	1.03	3

Heel contact reading for all subjects

# RESULTS – GAIT DATA

Subject	Standard value (N/kg)	Reading value (N/kg)	Percentage difference (%)
1	11	10.16	8
2	11	10.08	8
3	11	9.96	9
4	11	10.02	10
5	11	10.77	2
6	11	10.43	5
7	11	10.72	3
8	11	10.17	8
9	11	10.28	7
10	11	10.37	6

Maximum weight acceptance data

Subject	Standard value (N/kg)	Reading value (N/kg)	Percentage difference (%)
1	7	6.86	2
2	7	6.97	0
3	7	5.7	9
4	7	6.37	9
5	7	7.34	5
6	7	7.54	8
7	7	6.94	1
8	7	7.06	1
9	7	7.16	2
10	7	7.28	4

Mid-stance data

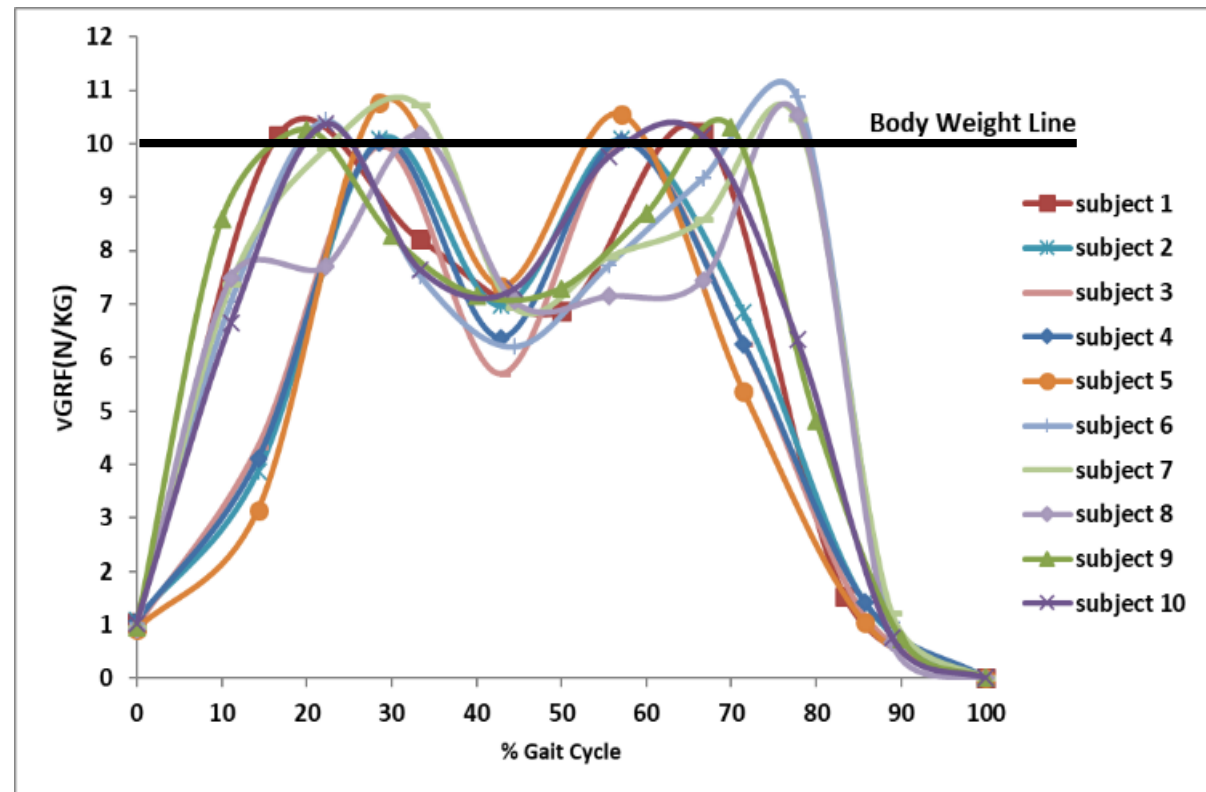
# RESULTS – GAIT DATA

Subject	Standard value (N/kg)	Reading value (N/kg)	Percentage difference (%)
1	11	10.23	7
2	11	10.09	7
3	11	10.04	9
4	11	10.05	9
5	11	10.55	4
6	11	10.88	1
7	11	10.46	5
8	11	10.53	4
9	11	10.31	6
10	11	10.14	8

Push-off Data



# RESULTS – vGRF Data



vGRF graph of 10 different subjects

# DISCUSSION

- In general the vGRF patterns for all subjects exhibited the similar curve pattern as the standard vGRF.
- For each of the gait events showed a significant different but still in the acceptable range - based on the fact that the percentage difference between the measured and the standard gait data is less than 10% for each of the observed gait event.
- In average the percentage difference is 5.5%, thus, this device is 94.5% accurate.
- Factors that can affect the accuracy of the device:
  - i. The variability of the style of walking between the subjects.
  - ii. The style of walking of an individual is greatly influenced by the body mass index (BMI), walking speed, stride length.

# CONCLUSION

- The development of the gait analysis device based on vGRF - shown a great potential to be further expanded in order to develop more accurate and cost effective device.
- This device has achieved 94.5% accuracy and shown a good repeatability.
- The accuracy of the device has been validated by comparing the result obtained from the experiment with standard gait pattern.
- In addition, all of the gait data can be transferred wirelessly and can be further analyzed to examine the performance of the gait.

# FUTURE WORK

- i. The analysis on longitudinal and lateral ground reaction forces.
- ii. Improved the performance of the device by conducting an experiment involving subject from different BMI – overweight and obese subjects; different types of activities – stairs ascending and descending.
- iii. Substitute manual computation that is believed can reduce the computation time and error in analyzing the gait data.

# Thank You